1	April 1, 2014-01-12
2	
3	JAB_2013_0239.R1
4	
5	
6	Changes in sagittal plane kinematics with treadmill familiarisation to
7	barefoot running
8	
9	
10	Authors: Isabel S Moore <sup>1</sup> and Sharon J Dixon <sup>2</sup>
11	<sup>1</sup> Sports injury Research Group, Cardiff School of Sport, Cardiff Metropolitan
12	University, Cardiff, Wales, UK
13	<sup>2</sup> Bioenergetics and Human Performance Research Group, Sport and Health
14	Sciences, University of Exeter, Exeter, UK
15	
16	Funding: No funding was received for this study.
17	Conflict of Interest Disclosure: No conflict of interest.
18	Corresponding author: Isabel Sarah Moore
19	
20	Address for correspondence: Isabel S. Moore, Cardiff School of Sport, Cardiff
21	Metropolitan University, Cyncoed, Cardiff, CF23 6XD
22	Email address: imoore@cardiffmet.ac.uk
23	Tel: +44 (0)29 6890 ext: 6342 Fax: +44 (0)29 2041 6895
24	
25	

## 26 Abstract

27 Interest in barefoot running and research is growing. However a methodological issue 28 surrounding investigations is how familiar the participants are with running barefoot. 29 The aim of the study was to assess the amount of time required for habitually shod 30 runners to become familiar with barefoot treadmill running. Twelve female 31 recreational runners, who were experienced treadmill users, ran barefoot on a 32 treadmill for 3x10 minutes at a self-selected speed, with 5 minute rest periods. 33 Sagittal plane kinematics of the hip, knee, ankle and foot during stance were recorded 34 during the first and last minute of each 10 minute bout. Strong reliability (ICC > 0.8) 35 was shown in most variables, after 20 minutes of running. Additionally, there was a 36 general trend for the smallest standard error of mean to occur during the same period. 37 Furthermore there were no significant differences in any of the biomechanical 38 variables after 20 minutes of running. Together this suggests that familiarisation was 39 achieved between 11 and 20 minutes of running barefoot on a treadmill. 40 Familiarisation was characterised by less plantarflexion and greater knee flexion at 41 touchdown. These results indicate that adequate familiarisation should be given in 42 future studies prior to gait assessment of barefoot treadmill running.

### Keywords: Kinematics, reliability, running gait

43 Word count: 3625

Л	1	
	-4-	

### Introduction

45 Currently there is great interest within the running community in running 46 barefoot (or in shoes mimicking barefoot running), with approximately 75% of American runners interested in it, from both a performance and injury perspective<sup>1</sup>. 47 48 Consequently, research into barefoot running has typically addressed its potential to enhance performance  $^{2-5}$  and reduce injury  $^{5-7}$ . Barefoot running is also utilised as a 49 50 test condition by many researchers investigating the effect of footwear, even though 51 for many participants it is likely to be the first time they have ever run barefoot. This 52 raises one of the methodological issues surrounding the study of barefoot running i.e. 53 the familiarity of the participants to running barefoot. A lack of familiarity may limit 54 the reliability of data obtained from a barefoot running condition.

55 Previous investigations assessing overground or treadmill running gait fall into 56 three categories regarding their barefoot/treadmill familiarisation procedures: 1) They fail to report whether any time was given for barefoot or treadmill familiarisation<sup>2-</sup> 57 <sup>4,8,9</sup>; 2) They state practice barefoot trials  $^{10,11}$  / treadmill familiarisation  $^{2,12,13}$  was 58 59 performed without specifying time; 3) They report familiarisation was achieved when the participant believed they were comfortable with the condition <sup>14-16</sup>. Given that 60 61 many studies find biomechanical differences between barefoot and shod conditions whilst running (e.g.<sup>11,17,18</sup>), it is possible that some findings may be influenced by 62 63 initial adjustments made in response to the removal of footwear if inadequate 64 familiarisation was given.

It has been argued that multiple steps need to be accumulated prior to biomechanical analysis of barefoot running <sup>12</sup>, so any gait modifications precede the gait assessment. However, the time necessary for runners to become familiar with barefoot running on a treadmill, such that their running kinematics stabilise to an

69	acceptable level during a testing session <sup>19,20</sup> , is unknown. Previous research
70	suggested that 8-9 minutes is required for spatio-temporal adjustments whilst running
71	shod on a treadmill <sup>19,21</sup> . A more recent study has demonstrated that kinematic
72	alterations can be made within six minutes of treadmill running $^{20}$ and that just 8
73	seconds is needed for kinetic familiarity <sup>22</sup> . These studies suggest the time taken for
74	shod individuals to adjust to one unfamiliar factor, treadmill running, is within 10
75	minutes. By using individuals who are already familiar with treadmill running, only
76	one unfamiliar factor exists when assessing barefoot treadmill running. Furthermore
77	barefoot running is often seen as another type of footwear condition by researchers,
78	implying kinematic responses to adjusting to such a test condition may be similar.
79	Therefore it is possible that the length of time required for barefoot familiarisation
80	might be similar to shod running, however this requires specific investigation.
81	The aim of this study was to assess the amount of time required for habitually
82	shod runners, with previous treadmill running experience, to become familiar with
83	barefoot treadmill running. It was hypothesised that runners would be able to produce
84	a consistent gait pattern within 10 minutes of running barefoot on a treadmill.
85	
86	Methods
87	
	Participants
88	<b>Participants</b> Twelve female recreational runners (height: $167.7 \pm 6.5$ cm; mass: $61.4 \pm 5.5$
88 89	
	Twelve female recreational runners (height: $167.7 \pm 6.5$ cm; mass: $61.4 \pm 5.5$

92 minutes per week on a treadmill for the past 6 months. All participants were free from

93 injury at the time of testing. Only runners who had limited (less than 5 minutes) or no

94 previous experience of barefoot running were included in the study. Thus all 95 participants were classified as beginner barefoot runners. Ethical approval was 96 obtained from the University's Sport and Health Sciences department.

97 Apparatus

An eight camera Peak Motus motion analysis system (Vicon Peak, 120 Hz, automatic optoelectronic system; Peak Performance Technologies, Inc., Englewood, CO), situated in an oval shape around a treadmill was used to capture 3D kinematic data (120 Hz). The system was calibrated using a wand length of 0.93 m and a fixed volume covering the treadmill belt.

103 A motorized treadmill (PPS 43med; Woodway, Weilam Rhein, Germany) was 104 used during the running trials. The speed of the treadmill was checked prior to testing 105 by recording the time taken for the treadmill belt to complete four revolutions. This 106 was captured using a Basler camera (100 Hz), which was positioned directly in front 107 of the treadmill, approximately 1.5 m away from the treadmill. The treadmill belt 108 length (3.60 m) was used to calculate the speed of the treadmill belt during four 109 revolutions. This speed was then compared to the digital display on the treadmill 110 monitor. This was completed for speeds ranging from 2.08 to 3.08 m s<sup>-1</sup> (mean:  $2.58 \pm$  $0.3 \text{ m}\cdot\text{s}^{-1}$ ). Based on the standard error of estimate there was 95% confidence that the 111 speed of the treadmill belt was within  $0.03 \text{ m} \cdot \text{s}^{-1}$  of the speed displayed on the 112 113 monitor.

114

# Marker Placement

115 Ten spherical reflective markers (diameter: 12 mm) were affixed to the right 116 lower limb of the participant using double-sided adhesive tape. A modified Soutas-117 Little <sup>23</sup> model was used to include the thigh segment, with markers placed on the 118 following anatomical landmarks: the proximal greater trochanter (hip); the medial and

119 lateral condyles (knee); midline of the posterior shank; the musculotendinous junction 120 where the medial and lateral belly of the gastrocnemius meet the Achilles tendon; the 121 mid-tibia below the belly of the tibialis anterior; the lateral malleolus (ankle); the 122 superior and inferior calcaneus; and the proximal head of the third metatarsal.

To determine stance a triaxial accelerometer (Trigno Wireless EMG, Delsys, Boston, MA, USA), sampling at 148 Hz, was affixed to the right heel of the participant's foot. The vertical component of the accelerometer data was used to detect touchdown (TD) and toe-off (TO), following similar procedures to those used elsewhere<sup>24</sup>.

## 128 **Procedures**

129 Each participant was instructed to self-select a speed which they felt they 130 could comfortably run at for 30 minutes and which was representative of their training 131 speed. They performed a warm-up on the treadmill for 5 minutes at this speed whilst 132 wearing their own, traditional, trainers. Then they ran barefoot at this speed for  $3 \times 10$ 133 minutes, with 5 minute rest periods in between each bout. This amount of time was chosen based on previous treadmill familiarisation studies<sup>19-21</sup>. As barefoot running 134 135 could potentially cause discomfort during initial runs the protocol included rest 136 periods to decrease the continuous time performing an unfamiliar task. No verbal 137 instructions were given to the participants with regards to running technique 138 throughout the testing period.

Data were captured in the first and last minute of each bout of 10 minutes, with the data being recorded during the first minute approximately 10 s after the treadmill had reached the required speed. This resulted in six time points: 1<sup>st</sup> minute (T1), 10<sup>th</sup> minute (T2), 11<sup>th</sup> minute (T3), 20<sup>th</sup> minute (T4), 21<sup>st</sup> minute (T5) and 30<sup>th</sup> minute (T6). Six complete, consecutive running cycles were collected during each

recording with only data during the stance period used for further analysis due to lossof data, particularly of the shank, during the swing phase.

146Data reduction

147 The coordinate data of the right leg were smoothed within the Peak Motus 148 software using a quintic spline smoothing technique. Further analysis occurred 149 through a customized MatLab (Math Works Inc., Cambridge, MA, USA) script. The 150 accelerometer data, which was simultaneously recorded alongside the kinematics, was 151 resampled to match the kinematic data collection frequency. Sagittal plane kinematics have the greatest reliability compared to the transverse and frontal planes <sup>25,26</sup>. 152 153 Therefore only sagittal plane movements were analysed. The hip angle was defined as 154 the angle between the thigh segment and the vertical line through the hip marker. The 155 knee angle was defined between the thigh and shank segments and the ankle angle 156 defined between the shank and foot segments. The foot angle was defined as the angle 157 between the ground and the vector created between the inferior calcaneus and the proximal head of the third metatarsal <sup>27</sup>. In addition to the running data, a standing 158 159 trial was recorded. This was performed in the anatomical position and the standing 160 trial angles were subtracted from the experimental data to provide anatomically 161 meaningful angles.

Positive values represent hip extension, knee flexion and ankle plantarflexion. The angles at TD and TO were calculated for the hip, knee and ankle, and foot angle at TD was used to detect footstrike patterns <sup>27</sup>. Additionally, the hip angle at 50% of stance (midstance) and the peak flexion during stance for both the knee and ankle were determined. Stride length was calculated using the following formula:

167 
$$SL = V x ST$$

168 SL = stride length. V = velocity of treadmill. ST = stride time (the time taken between 169 successive contacts of the right foot)  $^{21}$ .

170 Statistical analysis

171 Means were computed at each time point (T1, T2, T3, T4, T5 and T6), using 172 the six gait cycles recorded at that time point. Sharipo-Wilk tests were performed on 173 these means to test for normality and all were normally distributed. All within-subject 174 reliability tests of the dependent variables were calculated with these means. First, 175 intraclass correlation coefficients (ICC) between consecutive time points (T1-T2, T2-176 T3, T3-T4, T4-T5 and T5-T6) were established using the means calculated. Secondly, 177 using the same means the standard error of means (SEM) was computed, both in 178 absolute and relative terms. Finally, a one-way repeated measures ANOVA was used 179 to determine if there were any within-subject significant differences in each 180 dependent variable across the time points, with T-tests used for post-hoc comparisons 181 (Fisher's LSD). Statistical significance was set at  $p \le 0.05$  and all statistical tests were 182 performed using SPSS version 19 (SPSS Inc., Chicago, IL).

183

184

# Results

185 The intraclass correlations indicated that the highest reliability was found in 186 the last 10 minute cycle of barefoot running. All variables except knee flexion at TD 187 showed strong reliability (ICC > 0.8) after 20 minutes of running. Moderate reliability 188 (ICC: 0.6 - 0.8) was shown for all variables after 10 minutes of running barefoot. The 189 most consistent kinematics (ICC > 0.8) throughout the whole run were: foot at TD; 190 dorsiflexion at TD; hip at TD; hip at midstance; hip at TO and peak knee flexion. 191 Additionally stride length was found to have the highest ICC at each time period 192 during the 30 minutes.

There was a general trend for the smallest SEM, both in relative and absolute terms, to be found after 20 minutes of running. The only exceptions to this were the peak knee flexion and the hip at TD (Table 1), whereby the smallest SEMs were recorded during the first 10 minutes. However the relative SEMs were always below 10% for both variables, suggesting that these were the most reliable kinematics throughout the whole run.

There were four kinematic variables (out of 13) that were significantly different across time periods (Figure 1): dorsiflexion at TD; knee flexion at TD; knee flexion at TO; and hip angle at TO. Post hoc analysis revealed that there were no significant differences after T4, suggesting that the kinematic variables were stable after 20 minutes of running barefoot. No significant differences were observed in the other kinematic variables or the stride length.

205 In light of the change in ankle angle and unchanged foot angle, the tibia would need to be rotated further forward after the 20<sup>th</sup> minute, rather than the foot being 206 207 placed flatter to the ground. To test this hypothesis further analysis was performed on 208 the data to see if there was a significant change in the position of the shank segment 209 relative to the vertical at TD. This was performed using a one-way repeated measures 210 ANOVA, with the shank angle at TD as the dependent variable, followed by post-hoc 211 T-tests (Fishers' LSD). Results revealed a significant increase (19.9%; p = 0.022) in 212 the shank angle with the vertical at TD from T1 to T4 (11.9 vs. 14.2°, respectively). 213 Furthermore, there were no significant changes after 20 minutes.

214

215

### Discussion

This study investigated the time required for habitually shod runners to become familiar with barefoot treadmill running. The results show that kinematic

Human Kinetics, 1607 N Market St, Champaign, IL 61825

218 familiarisation occurred between 11 and 20 minutes of running, thus contradicting the 219 study hypothesis that less than 10 minutes would be required. There were no 220 significant differences in any of the biomechanical variables after 20 minutes (T1 to 221 T4), suggesting that the runners were able to produce a consistent gait pattern 222 following this period of time. Furthermore, all but one of the variables measured were 223 found to have strong reliability, based on ICC values, between 20-21 minutes and 21-224 30 minutes. Additionally, the smallest SEMs were found during the same time 225 periods.

226 Previous studies have reported that less time is required to become familiar with shod treadmill running, in the region of 6-9 minutes <sup>19-21</sup>. However it is likely 227 228 that the participants in these studies were habitual shod runners, meaning they only 229 had to adjust to the movement of the treadmill. The current study results suggest that 230 adjusting to the lack of footwear requires more time and is perhaps more complex 231 than only adjusting to the movement of a treadmill. The results also highlight that 232 researchers need to give participants appropriate familiarisation time before using 233 barefoot running as a test condition. This is due to the initial adjustments that 234 participants may be making to the lack of footwear, which for most is an unfamiliar 235 feeling.

Part of this unfamiliar feeling when running barefoot stems from the heightened somatosensory feedback that runners feel due to the lack of an external cushioning layer  $^{28-30}$ . Such a layer insulates the foot from its own sensory feedback that helps govern the impact during ground contact  $^{28,31}$ . It is argued that gait adjustments made during barefoot running attenuate mechanical stresses placed upon the feet  $^{28}$ , but the current findings suggest that such modifications to a runner's gait are not instantaneous. It is also conceivable that the reduced variability in running

243 mechanics could be a result of increased muscular fatigue and/or lower limb soreness 244 that would take time to develop. Whilst this study is unable to attribute the reduced 245 variability in running mechanics to a specific mechanism, based on the findings, it can 246 be advised that adequate familiarisation of between 11 and 20 minutes should be 247 given to habitually shod runners prior to testing barefoot treadmill running.

248 The variation (represented by the SD), particularly at the ankle angle during 249 initial ground contact (Figure 1a), could suggest that even though the mean for each 250 kinematic adjustment tended to plateau between 20 and 30 minutes (T4 and T6), there 251 was still large intra-individual variation during this time period. However Figure 2 252 indicates that this is not the case. The variation demonstrated was a result of large 253 inter-individual differences in ankle angle at TD, rather than intra-individual 254 differences. The lack of intra-individual differences suggests that runners were able to 255 perform a consistent gait pattern, hence were familiarised with barefoot treadmill 256 running, within 20 minutes of running.

257 As well as providing evidence regarding the time taken to adjust to barefoot 258 running, the current study highlights some interesting specific gait adjustments made from the first minute to the 20<sup>th</sup> minute. Firstly, runners adopted less plantarflexion 259 (or more dorsiflexion) following the 20<sup>th</sup> minute familiarisation (2.86 vs. -0.61°, T1 260 261 vs. T4 respectively). Initially 9 runners had at least 1° or more of plantarflexion at TD 262 compared to after 20 minutes when only 3 runners exhibited plantarflexion. This 263 suggests that some of the previously reported TD ankle angles, showing more plantarflexion when barefoot compared to shod, <sup>2,11</sup> could be a result of unfamiliarity 264 265 with barefoot running. It has been argued that such gait alterations reduced high loads 266 at the heel by increasing the contact area of the heel through a flatter foot at impact <sup>2,11</sup>. However the current study has demonstrated that this may be a natural response 267

to running barefoot for the first time and could be a result of inadequate familiarisation. As recent evidence has shown that a flatter foot placement reduces the peak heel pressures <sup>32</sup>, the fact that foot angle did not change during the familiarisation period, contradicting Squadrone and Gallozzi <sup>2</sup> and de Wit and colleagues <sup>11</sup>, suggests that there was no increase in contact area to disperse the impact load. Other kinematic changes could help explain the cushioning characteristics of barefoot running.

275 The initial average foot angle during familiarisation suggested that, generally, runners were midfoot striking during both the  $1^{st}$  (4.37°) and  $20^{th}$  minute (5.41°)<sup>22</sup>. 276 Based on the classification of Altman and Davis  $^{27}$  (forefoot striking: foot angle < -277 278 1.6°; rearfoot striking: foot angle > 8°; midfoot striking:  $-1.6^{\circ}$  < foot angle < 8°) there 279 were 3 forefoot strikers, 5 midfoot strikers and 4 rearfoot strikers. Whilst foot angle 280 remained similar across the different time points, there were changes in the shank 281 angle relative to the vertical. This tibial movement would explain the greater knee 282 flexion recorded at TD with increased running familiarity, consistent with the hip 283 angle at TD being similar across each time point. Previous research has reported 284 either greater knee flexion at TD when running barefoot compared to running shod <sup>11,33</sup> or no difference between the two conditions <sup>2</sup>. However, the current findings 285 286 suggest adequate familiarisation allows runners to produce even greater knee flexion 287 at TD meaning previous differences found may be smaller than what could have been 288 achieved with familiarisation. Furthermore de Wit and colleagues calculated that 96% 289 of the variance in foot angle at TD could be determined by the ankle angle and shank 290 angle during barefoot running <sup>11</sup>, showing how intrinsically linked these positional 291 angles are. Therefore, it appears that with increased familiarity runners utilise the 292 knee to a greater degree to help attenuate the impact by reducing their effective mass

<sup>34</sup>. By adopting a more flexed knee at TD the magnitude of impact force experienced could be reduced <sup>35</sup>, possibly reducing the likelihood of injury <sup>36</sup>. So rather than producing a flatter foot, increasing the amount of contact area to lower the loads experienced, it seems that runners tended to change their knee and shank positions to possibly facilitate a reduction of impact force.

298 Stride length was the most reliable gait characteristic with little variation over 299 time, meaning runners adjusted their stride length almost instantaneously at the 300 beginning of the run. Therefore it is likely that the shorter stride lengths reported during barefoot running<sup>2,5,11</sup> may be an anticipatory strategy, such as that used when 301 adjusting leg stiffness in response to changes in surface <sup>37</sup>. This strategy would be 302 303 controlled by visual cues of the surface, knowledge of the surface properties from previous experiences <sup>37</sup>, and heightened somatosensory feedback whilst standing on 304 305 the surface prior to running on it, due to the lack of an external layer between the foot 306 and surface. Previous results have shown that even a small layer between the foot and 307 the surface that lessens somatosensory feedback, such as a minimalist shoe, means runners choose a similar stride length to that demonstrated during shod running  $^2$ . For 308 309 such a stride length to be consistently reproducible during shod running on a treadmill may take between 2-4 minutes <sup>20</sup>. Conversely by removing the external layers that 310 311 insulate the foot from impact with the ground, runners are able to adopt consistent 312 stride lengths almost immediately. It is important to note, that although the results 313 show stride length to be adopted instantaneously, we cannot discern whether these 314 stride lengths were different to the habitual shod stride lengths of the runners.

315 Due to this heightened somatosensory feedback when running barefoot the 316 interaction between the surface and the foot should play a greater role in determining 317 the running mechanics of an individual. Elements known to affect a runner's gait,

such as surface stiffness <sup>37,38</sup>, could influence the time to familiarisation. The same 318 319 treadmill was used throughout testing to minimise the effect the surface could have on 320 time to familiarisation, but caution should be exercised when generalising these 321 findings to other treadmills and overground running with different surface properties. Nevertheless, the results support the argument made by Divert et al., <sup>12</sup> that multiple 322 323 steps need to be accumulated prior to assessing the biomechanics of barefoot running. 324 Therefore it is not unreasonable to suggest that numerous practice trials should be 325 given in barefoot overground running conditions prior to experimental testing. 326 However, further research is needed to assess the time/number of trials required.

327 It is possible that familiarisation may have occurred sooner than 20 minutes if 328 no rest period was given. However this protocol was deemed necessary following 329 pilot work, which tested 30 minutes of continuous running and found this caused 330 soreness in the lower limb during and post-exercise. For this reason, researchers 331 should be cautious about familiarising participants to barefoot treadmill running the 332 same day as their experimental testing. Whilst slight alterations to running mechanics 333 may occur in the initial few minutes of treadmill running performed on separate days, 334 providing runners with adequate familiarisation to treadmill running on a separate 335 day, prior to testing, has been shown to reduce these alterations to running mechanics 336 <sup>19</sup>. Additionally, familiarisation could have occurred at any point between 11 and 20 337 minutes. However, due to data being collected at the beginning and end of each bout, 338 the exact time of familiarisation cannot be identified. Further investigations, which 339 record data more frequently, are needed to ascertain the exact minute adequate 340 familiarisation was achieved.

In conclusion, to familiarise habitually shod, experienced treadmill runners tobarefoot treadmill running, 11 to 20 minutes of running on a treadmill should be given

343 in one session. Kinematic and spatio-temporal measures were consistent and stable 344 within 20 minutes, suggesting that future studies should include a sufficient period of 345 familiarisation to barefoot running prior to commencing experimentation. After 346 familiarisation, runners adopted less plantarflexion and greater knee flexion during 347 initial ground contact. However stride length changes during barefoot running were 348 adopted immediately. 349 References 350 351 1. Rothschild CE. Primitive running: a survey analysis of runners' interest, 352 participation, and implementation. J Strength Con Res. 2012;26(8):2021-2026. 353 2. Squadrone R, Gallozzi C. Biomechanical and physiological comparison of 354 barefoot and two shod conditions in experienced barefoot runners. J Sports Med P Fitness. 2009;49(1):6-13. 355 356 Perl DP, Daoud AI, Lieberman DE. Effects of footwear and strike type on 3. 357 running economy. Med Sci Sports Exerc. 2012;44(7):1335-1343. 358 4. Franz JR, Wierzbinski CM, Kram R. Metabolic cost of running barefoot 359 versus shod: is lighter better? Med Sci Sports Exerc. 2012;44(8):1519-1525. 360 5. Moore IS, Jones AM, Dixon SJ. The pursuit of improved running 361 performance: Can changes in cushioning and somatosensory feedback 362 influence running economy and injury risk? Footwear Sci. 2014;6(1):1-11. 363 6. Giuliani J, Masini B, Alitz C, Owens BD. Barefoot-simulating footwear 364 associated with metatarsal stress injury in 2 runners. Orthopedics. 365 2011;34(7):e320-323.

- 366 7. Daoud AI, Geissler GJ, Wang F, Saretsky J, Daoud YA, Lieberman DE. Foot
- 367 strike and injury rates in endurance runners: a retrospective study. *Med Sci*368 *Sports Exerc.* 2012;44(7):1325-1334.
- Barnes A, Wheat J, Milner CE. Use of gait sandals for measuring rearfoot and
   shank motion during running. *Gait Posture*. 2010;32(1):133-135.
- Hanson NJ, Berg K, Deka P, Meendering JR, Ryan C. Oxygen cost of running
  barefoot vs. running shod. *Int J Sports Med.* 2011;32(6):401-406.
- 373 10. Stacoff A, Nigg BM, Reinschmidt C, van den Bogert AJ, Lundberg A.
- 374 Tibiocalcaneal kinematics of barefoot versus shod running. *J Biomech*.
  375 2000;33(11):1387-1395.
- 376 11. De Wit B, De Clercq D, Aerts P. Biomechanical analysis of the stance phase
  377 during barefoot and shod running. *J Biomech.* 2000;33(3):269-278.
- Divert C, Mornieux G, Baur H, Mayer F, Belli A. Mechanical comparison of
  barefoot and shod running. *Int J Sports Med.* 2005;26(7):593-598.
- 380 13. Divert C, Baur H, Mornieux G, Mayer F, Belli A. Stiffness adaptations in
  381 shod running. *J Appl Biomech.* 2005;21(4):311-321.
- 382 14. Dixon SJ, McNally K. Influence of orthotic devices prescribed using pressure
- data on lower extremity kinematics and pressures beneath the shoe during
  running. *Clin Biomech.* 2008;23(5):593-600.
- Lilley K. Dixon, SJ, Stiles V. A biomechanical comparison of the running gait
  of mature and young females. *Gait Posture*. 2011;33(3):496-500.
- 387 16. Riley PO, Dicharry J, Franz J, Croce UD, Wilder RP, Kerrigan CD. A
- 388 kinematics and kinetic comparison of overground and treadmill running. *Med*389 *Sci Sports Exerc.* 2008;40(6):1093-1100.

- NcNair PJ, Marshall RN. Kinematic and kinetic parameters associated with
  running in different shoes. *Br J Sports Med.* 1994;28(4):256-260.
- 392 18. Sinclair J, Greenhalgh A, Brooks D, Edmundson CJ, Hobbs SJ. The influence
  393 of barefoot and barefoot-inspired footwear on the kinetcs and kinematics of
  394 running in comparison to conventional running shoes. *Footwear Sci.*395 2013;5(1):45-53.
- 396 19. Schieb DA. Kinematic accommodation of novice treadmill runners. *Res Q*397 *Exerc Sport.* 1986;57(1):1-7.
- 20. Lavcanska V, Taylor NF, Schache AG. Familiarization to treadmill running in
  young unimpaired adults. *Hum Movement Sci.* 2005;24(4):544-557.
- Cavanagh PR, Williams KR. The effect of stride length variation on oxygen
  uptake during distance running. *Med Sci Sports Exerc.* 1982;14(1):30-35.
- White SC, Gilchrist LA, Christina KA. Within-day accommodation effects on
  vertical reaction forces for treadmill running. *J Appl Biomech*. 2002;18(1):74-
- 404 82.
- Soutas-Little RW, Beavis GC, Verstraete MC, Markus TL. Analysis of foot
  motion during running using a joint co-ordinate system. *Med Sci Sports Exerc*.
  1987;19(3):285-293.
- 408 24. Sinclair J, Hobbs SJ, Protheroe L, Edmundson CJ, Greenhalgh A.
  409 Determination of gait events using an externally mounted shank
  410 accelerometer. *J Appl Biomec.* 2013;29(1):118-122.
- 411 25. Queen RM, Gross MT, Liu H-Y. Repeatability of lower extremity kinetics and
  412 kinematics for standardized and self-selected running speeds. *Gait Posture*.
  413 2006;23(3):282-287.

- 414 26. McGinley JL, Baker R, Wolfe R, Morris ME. The reliability of three-
- 415 dimensional kinematic gait measurements: A systematic review. *Gait Posture*.
  416 2009;29(3):360-369.
- 417 27. Altman AR, Davis IS. A kinematic method for footstrike pattern detection in
  418 barefoot and shod runners. *Gait Posture*. 2012;35(2):298-300.
- 419 28. Robbins SE, Hanna AM. Running-related injury prevention through barefoot
  420 adaptations. *Med Sci Sports Exerc.* 1987;19(2):148-156.
- 421 29. Robbins SE, Hanna AM, Gouw GJ. Overload protection: avoidance response
  422 to heavy plantar surface loading. *Med Sci Sports Exerc.* 1988;20(1):85-92.
- 423 30. Lieberman DE, Venkadesan M, Werbel WA, et al. Foot strike patterns and
  424 collision forces in habitually barefoot versus shod runners. *Nature*. Jan 28
  425 2010;463(7280):531-535.
- 426 31. Robbins SE, Gouw GJ, Hanna AM. Running-related injury prevention through
  427 innate impact-moderating behavior. *Med Sci Sports Exerc.* 1989;21(2):130428 139.
- 32. Nunns M, House C, Fallowfield J, Allsopp A, Dixon SJ. Biomechanical
  characteristics of barefoot strike modalities. *J Biomech.* 2013;46(15):26032610.
- 432 33. de Koning JJ, Nigg BM. Kinematic factors affecting initial peak vertical
  433 ground reaction forces in running. *J Biomech.* 1994;27(6):673-673.
- 434 34. Derrick TR. The effects of knee contact angle on impact forces and
  435 accelerations. *Med Sci Sports Exerc.* 2004;36(5):832-837.
- 436 35. Gerritsen KGM, van den Bogert AJ, Nigg BM. Direct dynamics simulation of
  437 the impact phase in heel-toe running. *J Biomech.* 1995;28(6):661-668.

438	36.	Ferber R, McClay-Davis I, Hamill J, Pollard CD, McKeown KA. Kinetic
439		variables in subjects with previous lower extremity stress fractures. Med Sci
440		Sports Exerc. 2002;34(5):S5.
441	37.	Ferris DP, Liang K, Farley CT. Runners adjust leg stiffness for their first step
442		on a new running surface. J Biomech. 1999;32(8):787-794.
443	38.	Dixon SJ, Collop AC, Batt ME. Surface effects on ground reaction forces and
444		lower extremity kinematics in running. Med Sci Sports Exerc.
445		2000;32(11):1919-1926.
446	Figur	e 1. Kinematic changes over time. a) Ankle at TD. b) Knee at TD. c) Knee at
447	TO. d	) Hip at TO. TD = touchdown. TO = toe-off.
448		
449	Figur	re 2. Individual ankle angles at TD across each time point (grey lines). The mean
450	value	s for each time point is represented by the black line ( $\pm$ SD). TD = touchdown.
451		
452		
453		
454		
455		
456		
457		
458		
459		
460		
461		
462		

and stride length					
Variable			Time periods		
	T1-T2	T2-T3	T3-T4	T4-T5	T5-T6
Foot angle TD <sup>a</sup>	1.20	1.82	1.63	1.41	0.99
Dorsiflexion TD <sup>a</sup>	2.87	2.55	2.03	1.82	1.19
Dorsiflexion peak	2.33 (17.5%)	4.35 (32.2%)	2.26 (18.1%)	1.12 (9.2%)	1.78 (14.5%)
Dorsiflexion TO <sup>a</sup>	7.17	7.15	3.33	2.71	2.10
Knee flexion TD	3.21 (30.6%)	2.00 (19.5%)	2.19 (19.6%)	2.22 (18.0%)	1.92 (15.2%)
Knee flexion peak	1.48 (4.0%)	2.81 (7.7%)	2.61 (7.2%)	2.72 (7.4%)	1.66 (4.4%)
Knee flexion TO	2.34 (18.2%)	1.52 (12.8%)	1.66 (13.4%)	1.46 (12.2%)	1.16 (9.8%)
Hip TD	0.59 (2.8%)	0.77 (3.8%)	0.91 (4.5%)	1.29 (6.3%)	0.69 (3.3%)
Hip midstance	1.63 (13.7%)	1.19 (10.0%)	1.07 (8.8%)	1.20 (10.2%)	0.80 (7.0%)
Hip TO	1.89 (10.3%)	1.96 (10.2%)	1.65 (9.0%)	1.39 (7.6%)	1.18 (6.2%)
Stride length	0.04 (1.7%)	0.04 (1.7%)	0.02 (1.0%)	0.02 (0.6%)	0.02 (0.6%)

463 **Table 1**. Absolute (relative) standard error of means (SEM) of the sagittal plane kinematics 464 and stride length

<sup>a</sup> Relative standard error of mean was not calculated due to the variation in kinematic values around

466 zero. T1 =  $1^{st}$  minute. T2 =  $10^{th}$  minute. T3 =  $11^{th}$  minute. T4 =  $20^{th}$  minute. T5 =  $21^{st}$  minute. T6 =  $30^{th}$ 

467 minute. TD = touchdown. TO = toe-off.

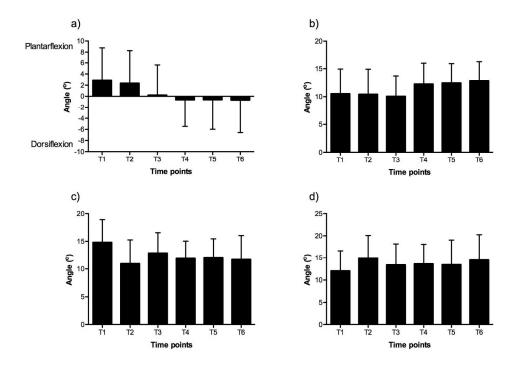


Figure 1. Kinematic changes over time. a) Ankle at TD. b) Knee at TD. c) Knee at TO. d) Hip at TO. TD = touchdown. TO = toe-off. 178x124mm (300 x 300 DPI)

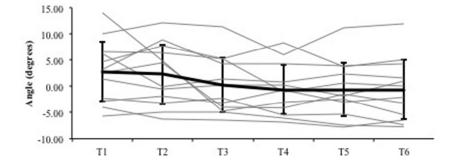


Figure 2. Individual ankle angles at TD across each time point (grey lines). The mean values for each time point is represented by the black line ( $\pm$ SD). TD = touchdown. 146x57mm (72 x 72 DPI)