1	The Future of Mechanical Circulatory Support
2	First Author: William K. Cornwell III MD, MSCS
3	Authors: William K. Cornwell III MD, MSCS ¹ ; Eric Stöhr PhD ^{2,3} ; Barry McDonnell PhD ² ;
4	Keith Aaronson MD, MS ⁴ ; Chris Hayward MD ⁵ ; Jay D. Pal MD, PhD ⁶ .
5	Author Affiliations:
6	1. Department of Medicine-Cardiology, University of Colorado Anschutz Medical
7	Campus, Aurora CO, USA.
8	2. School of Sport and Health Sciences, Cardiff Metropolitan University, CF5 2YB,
9	UK.
10	3. Department of Cardiothoracic Surgery, University of Colorado Anschutz Medical
11	Campus, Aurora CO, USA.
12	4. Division of Cardiovascular Medicine, University of Michigan, Ann Arbor MI, USA.
13	5. School of Medicine, University of New South Wales, Sydney, NSW, Australia.
14	6. Department of Cardiothoracic Surgery, University of Colorado Anschutz Medical
15	Campus, Aurora CO, USA.
16	Corresponding Author:
17	William K. Cornwell III MD, MSCS
18	Department of Medicine-Cardiology, University of Colorado Anschutz Medical
19	Campus
20	126312 E. 17 th Ave
21	B130, Office 7107
22	Aurora CO 80045
23	Ph: 303-724-2085; fax: 303-724-2094

24 william.cornwell@cuanschutz.edu

25 **Disclosures**:

26 Dr. Cornwell receives research funds from NIH/NHLBI (#1K23HLI32048), Medtronic Inc,

- 27 Bioventrix Inc, and Riva Inc. Dr. Cornwell is a consultant for Medtronic Inc and
- 28 Bioventrix Inc. Dr Hayward receives research support and has received consulting fees
- 29 / honoraria from Medtronic, Abbott, has research support in kind from BiVACOR and is
- 30 on the medical advisory board of Cardiobionic. Dr. Aaronson has received contracted
- research funding to the University of Michigan from Abbott and Bioventrix, honoraria
- 32 from Medtronic for participation on an Independent Physician Quality Panel, consulting
- fees from NuPulseCV and is on the scientific advisory board of Procyrion. Dr. Pal
- receives research support from Medtronic Inc and is a consultant for Medtronic Inc. Dr.
- 35 Stöhr and Dr. McDonnell report no disclosures.
- 36

37 Word Count: 1042

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Much has transpired in the world of mechanical circulatory support (MCS) in a 47 very short period of time. Less than twenty years ago, the pulsatile Heartmate XVE was 48 found to be superior to medical therapy for improving survival among patients with 49 advanced heart failure with reduced ejection fraction (HFrEF).¹ While simplistic in 50 design, the XVE was large, bulky, and unstable over the long-term. Innovative 51 52 approaches towards device design eventually led to the introduction of continuous-flow technology, first with the axial flow Heartmate II left ventricular assist device $(LVAD)^2$, 53 followed by two centrifugal-flow pumps, the Heartware VAD (HVAD)³ and the Heartmate 54 3.⁴ Over the last decade, healthy competition between these pumps spawned a 55 revolution in all aspects of MCS, from refinement of pump design, drivelines and 56 batteries, to automated modulations in speed, surgical implantation techniques, and 57 even the concept of LVADs as a "bridge-to-recovery". Survival and quality-of-life have 58 improved, and the rate of LVAD-associated complications has declined. Fast forward to 59 2021, whence one of these pumps – the Heartmate 3, has emerged victorious in this 60 competition, with the HVAD finishing as the "runner-up". Following withdrawal of the 61 HVAD from the global market on June 3rd, 2021, we are now left with one device – a 62 reliable pump, with which to incorporate into our armamentarium for managing patients 63 with advanced HFrEF. 64

65 Competition will always declare a victor, and while the Heartmate 3 will now 66 inevitably receive increasing levels of attention and scrutiny, there remains much to be 67 learned from the HVAD in spite of its shortcomings. The HVAD platform incorporated 68 unique features – namely, real-time waveform analysis and logfiles, not available on 69 other durable MCS devices, which improved patient care and general awareness of how

the cardiovascular system interacts with centrifugal-flow pumps. The flow waveform is a 70 real-time, continuous display of pump performance, a feature that allows for an 71 estimation of LVAD volume and pressure, analogous to ventricular pressure-volume 72 loops, the gold-standard method of characterizing ventricular function. These measures 73 allow clinicians to make informed decisions on management of patient factors such as 74 75 fluid status, blood pressure, arrhythmias and right heart function. Conditions such as overt right heart failure and pericardial tamponade can be identified by interrogation of 76 the waveform and logfiles. In addition to the Medtronic HVAD, the Abiomed Impella and 77 78 Abbott Centrimag system also utilize waveform displays, highlighting the importance of continuous evaluation of pump performance on all MCS platforms. 79

The potential for investigation of patient-pump interaction is the more interesting 80 application of the waveform. Physiologically responsive pumps are a holy grail of 81 durable MCS therapy. While current pumps allow for greater exercise tolerance 82 compared to the pre-implant state, recent analyses have demonstrated that patients still 83 have features of heart failure after LVAD implantation.⁵ Waveform analysis allowed 84 physicians to appreciate that a continuous-flow LVAD, operating at a fixed speed, does 85 not adequately perfuse the body during periods of increased demand, such as occurs 86 during exercise. Analogous to rate-responsive pacemakers, speed-modulating LVADs 87 can only be developed once the interaction between patient and LVAD is better 88 89 understood. While the HVAD was clinically limited by inferior outcomes, particularly in regards to survival and stroke rate, it nevertheless created a role for itself in the MCS 90 space that is not filled by the Heartmate 3. Instantaneous waveform display at the 91 92 patient's bedside proved to be an invaluable asset for clinical decision-making since it

provided information regarding factors such as heart rate and arrhythmia burden, 93 preload assessment, status of aortic valve opening and flow pulsatility. The graphical 94 logfile display provided additional information, including diurnal variations in pump 95 performance, flow pulsatility, suction, and even evidence of device-related 96 complications such as gastrointestinal bleeding. As such, certain aspects of the HVAD 97 98 proved invaluable to patient management and it is our hope that these attributes are incorporated as standardized features of future MCS platforms. Along those lines, the 99 question is, where to now? The challenge for providers is to derive as much information 100 101 as possible from the pump while also encouraging device engineers to push the envelope in design as newer pumps emerge. 102

Regardless of the device, LVAD patients – including those supported by the 103 Heartmate 3, are limited by complications including strokes, right heart failure, 104 gastrointestinal bleeding and device-related infections, which may occur in isolation, 105 sequentially or simultaneously. The mechanism(s) predisposing to these complications 106 - while not fully understood, may be related, at least in part, to a limitation of all 107 continuous-flow pumps, namely, the lack of a physiologic pulse. The relative 108 109 importance of pulsatility has long been debated amongst experts, however, the true flow profiles throughout the macro- and microcirculation of different LVAD patients largely 110 remain unknown. Patient-specific end-organ flow profiles result from an individual's 111 112 unique haemodynamic profile and are the product of contractile reserve of the native ventricle, flow through the pump itself, and interactions with the central and peripheral 113 arteries, which may be dysfunctional (e.g. endothelial dysfunction, arterial stiffness) as 114 part of the natural history of HFrEF. 115

A successful reduction in the rate of adverse events depends on the ability to 116 better understand the degree to which an LVAD can integrate into the cardiovascular 117 system. To this end, coordination between device manufacturers, clinical practitioners, 118 and researchers is paramount. Device manufacturers can facilitate immediate bedside 119 availability of pump behavior from the LVAD controller. In-vivo cardiovascular 120 121 hemodynamics and heart-pump interactions can be provided through invasive and noninvasive means in both clinical and research settings. Patient-specific profiles of flow 122 patterns should continue to be incorporated into bedside management to personalize 123 124 care.

HVAD engineers and developers are to be congratulated for their contributions to 125 the field of durable MCS. While this chapter in LVAD technology closes, and a new one 126 emerges – one involving a single device sitting comfortably with no immediate 127 competitor, we remember the irreplaceable value and lasting impression the HVAD has 128 had on the field. At the same time, the Heartmate 3 designers are to be congratulated 129 for earning their place at the head of the table. Moving forward, we must be careful to 130 avoid complacency with the field in its new state, which now involves a single pump. 131 Complacency leads to stagnation, which neither the field of MCS, nor its patients, can 132 afford. The competition between pumps created an environment that encouraged 133 tremendous innovation and improved outcomes. That competitive drive to excel must 134 135 continue.

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